

Nieinwazyjny monitoring we wczesnym wykrywaniu migotania przedsionków

Non-invasive Monitoring for Early Detection of Atrial Fibrillation

NOMED-AF

Projekt w ramach Strategicznego Programu Badań
Naukowych i Prac Rozwojowych - STRATEGMED II
Narodowe Centrum Badań i Rozwoju



NOMED-AF – Zadania ITAM

Opracowanie przenośnego urządzenia -
w postaci bransolety - wraz z wbudowanym
oprogramowaniem dla detekcji AF,
oraz wytworzenie produktu do badań klinicznych.

Ocena i optymalizacja czułości i swoistości
wykrywania AF przez proponowane urządzenie.

Założenia funkcjonalne urządzenia

- Łatwość aplikacji i obsługi urządzenia z uwzględnieniem jego przeznaczenia dla osób starszych (65+)
- Stabilność długoczasowego monitorowania (do 30 dni) bez utrudnień dla pacjenta
- Automatyczna detekcja AF w oparciu o rejestrowane sygnały biomedyczne
- Transmisja fragmentów sygnału EKG z wykrytymi epizodami AF do Centralnej Platformy Monitorującej – PMP (Patient Monitoring Platform) raz na dobę

Założenia konstrukcyjne urządzenia - ITAM

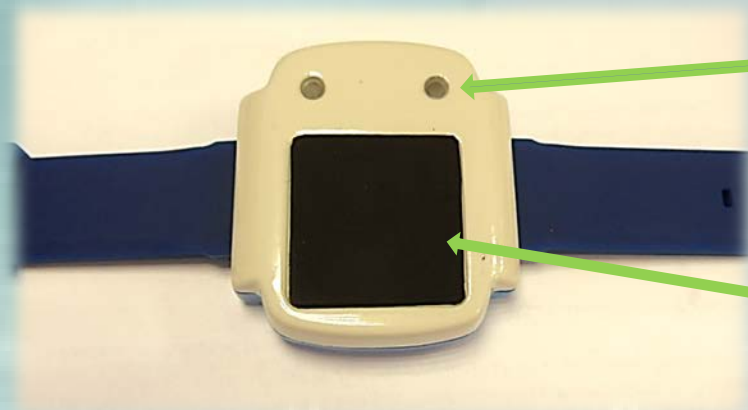
- Brak elektrod EKG naklejanych na skórę pacjenta
- wykonanie w formie ergonomicznej bransolety zakładanej na przegub ręki
- Moduł optycznego sensora do ciągłej rejestracji sygnału pletyzmograficznego – fali tętna
- Moduł do okresowej rejestracji sygnału EKG z elektrod kontaktowych
- Algorytm dwuetapowej detekcji i weryfikacji epizodów AF na podstawie sygnałów: pletyzmograficznego i EKG
- Sygnalizacja optyczna i wibroakustyczna zdarzeń wymagających reakcji pacjenta
- Zasilanie z baterii ładowalnej, zapewniające czas pracy do kolejnej zamiany urządzenia i ładowania, w cyklu 24-godzinny (pacjent otrzymuje dwa urządzenia)

Urządzenie: Bracel-AF



Urządzenie: Bracel-AF

Kluczowe elementy urządzenia: moduł sensora do ciągłej rejestracji sygnału pletyzmograficznego i elektrody do okresowej rejestracji sygnału EKG

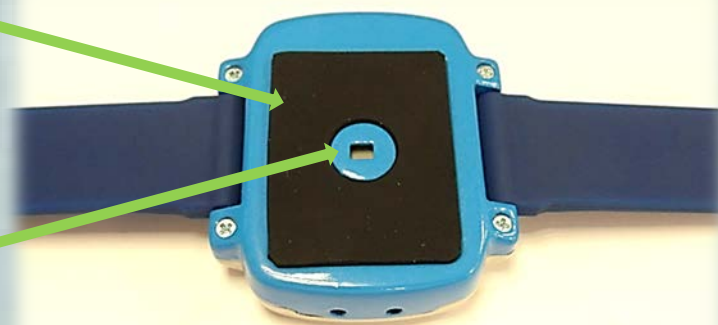


optyczne elementy
sygnalizacyjne

zewnętrzna
elektroda EKG

wewnętrzna
elektroda EKG

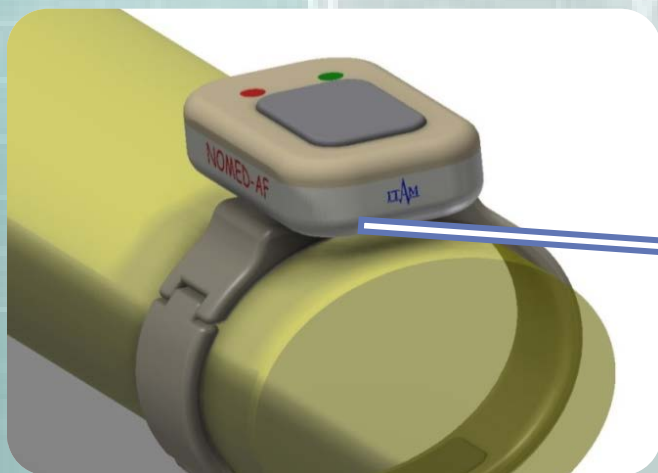
sensor
pulsoksymetryczny



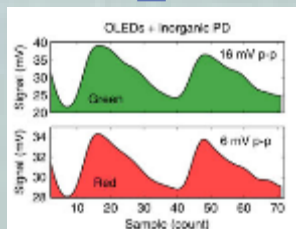
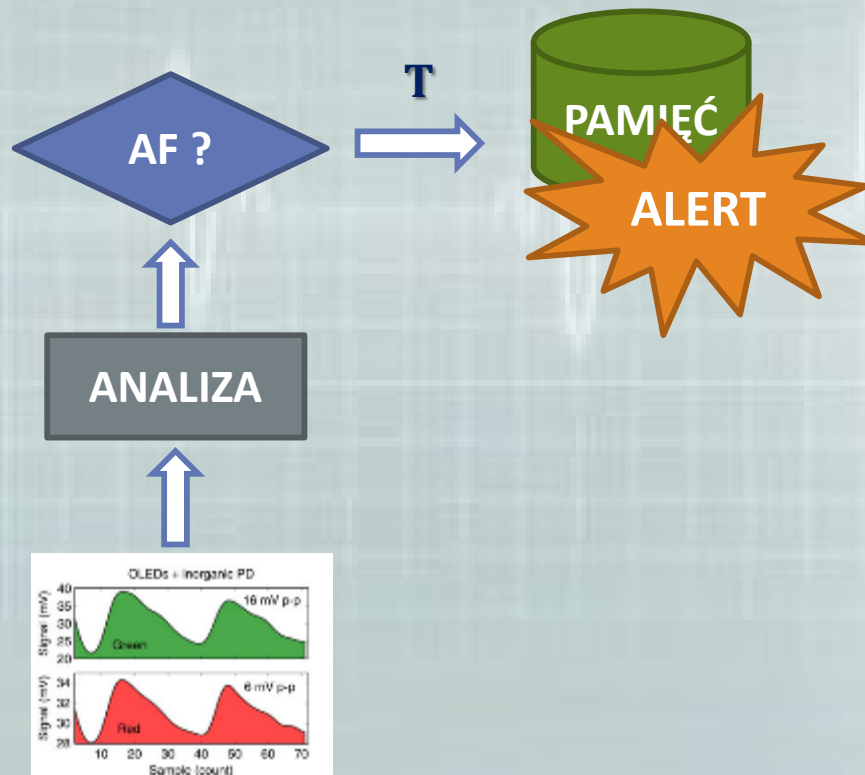
Scenariusz użycia urządzenia: Bracel-AF

Ciągła rejestracja sygnału pletyzmograficznego (PPG)

Detekcja epizodów - „podejrzenie wystąpienia AF”



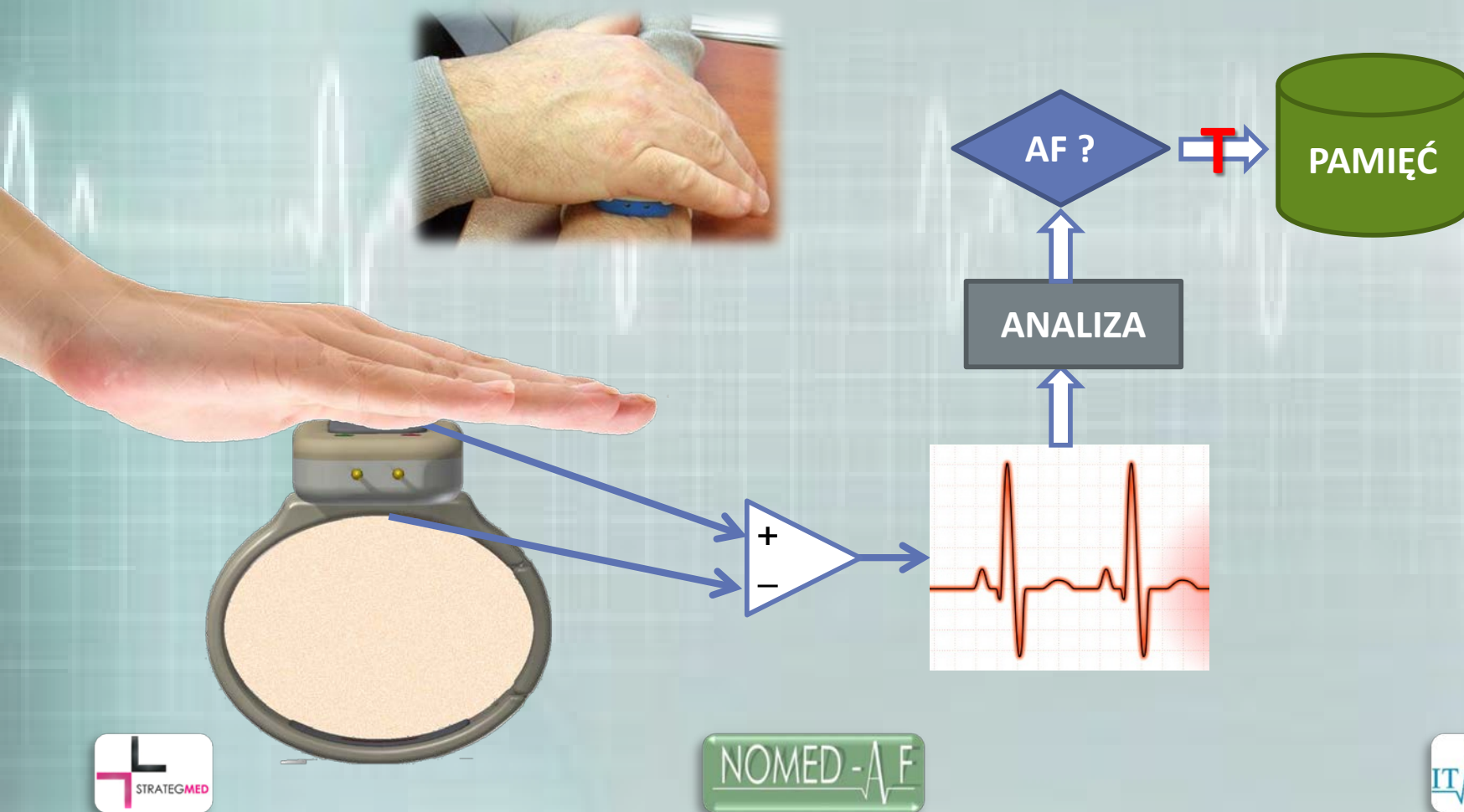
PPG



Scenariusz użycia urządzenia: Bracel-AF

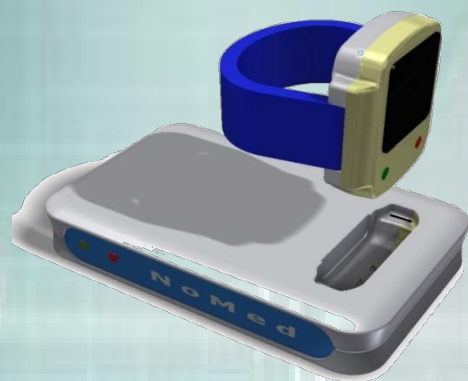
Epizodyczna rejestracja sygnału EKG

Weryfikacja wystąpienia AF



Scenariusz użycia urządzenia: Bracel-AF

Okresowa zamiana urządzenia (co 24h)
dla zapewnienia ciągłego monitorowania



PMP

GSM

Stacja dokująca:

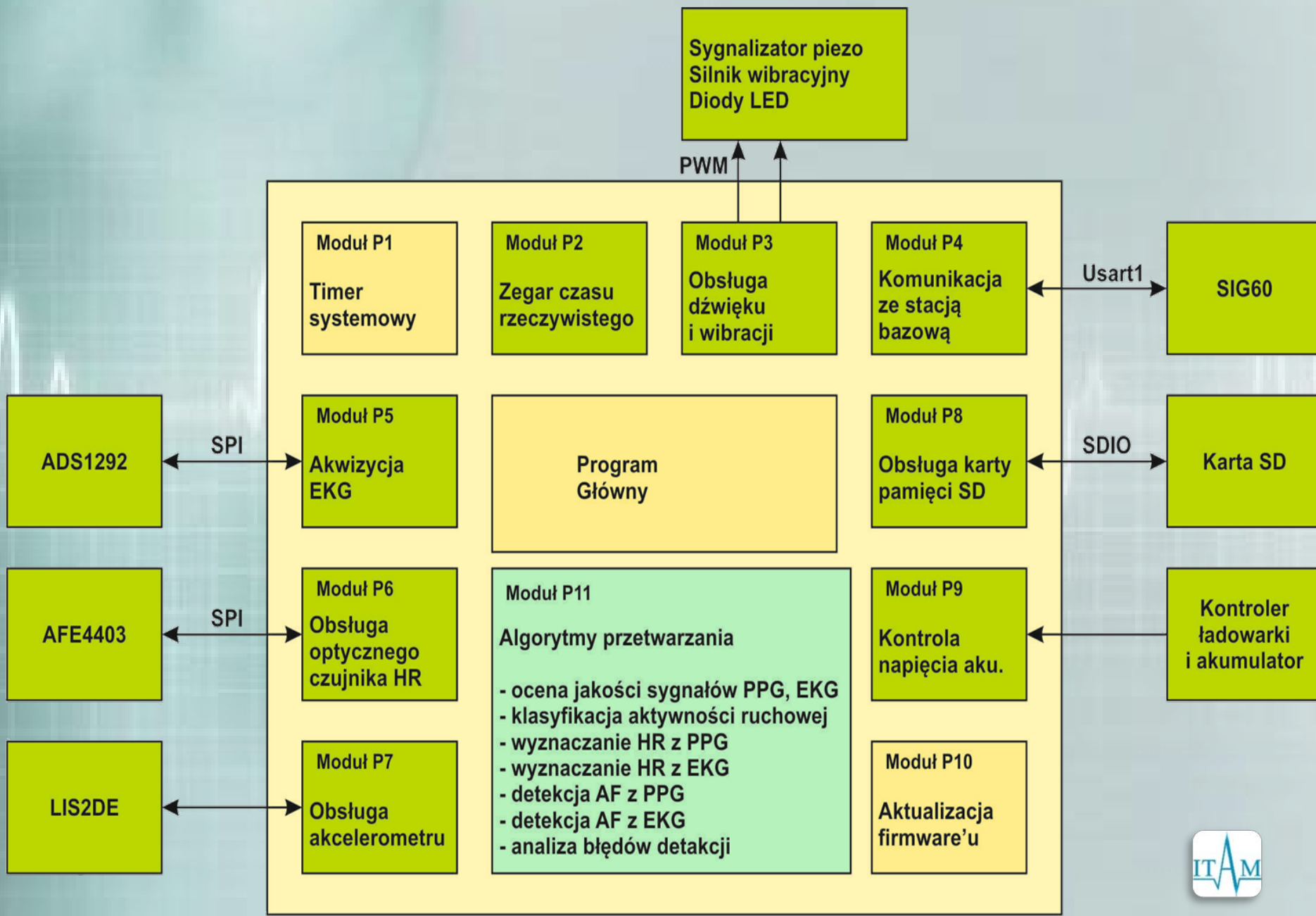
- ładowanie baterii
- odebranie danych z urządzenia i transmisja do PMP (Patient Monitoring Platform)

Płytką drukowaną z elementami elektronicznymi

4 cm

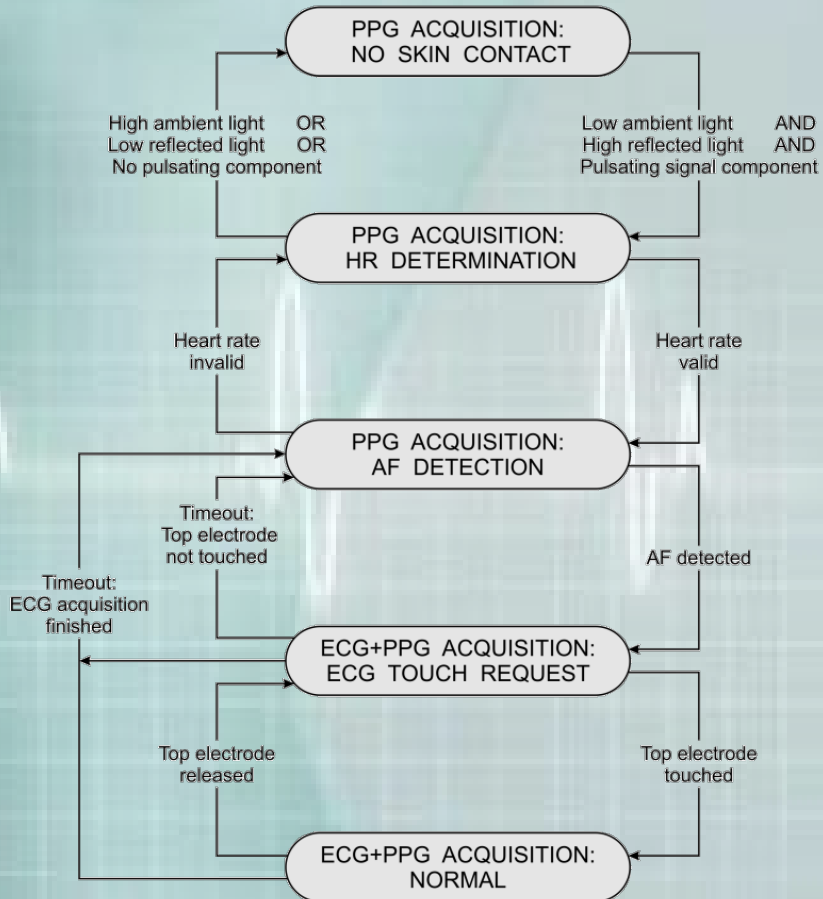


Schemat blokowy modułu elektroniki i oprogramowania

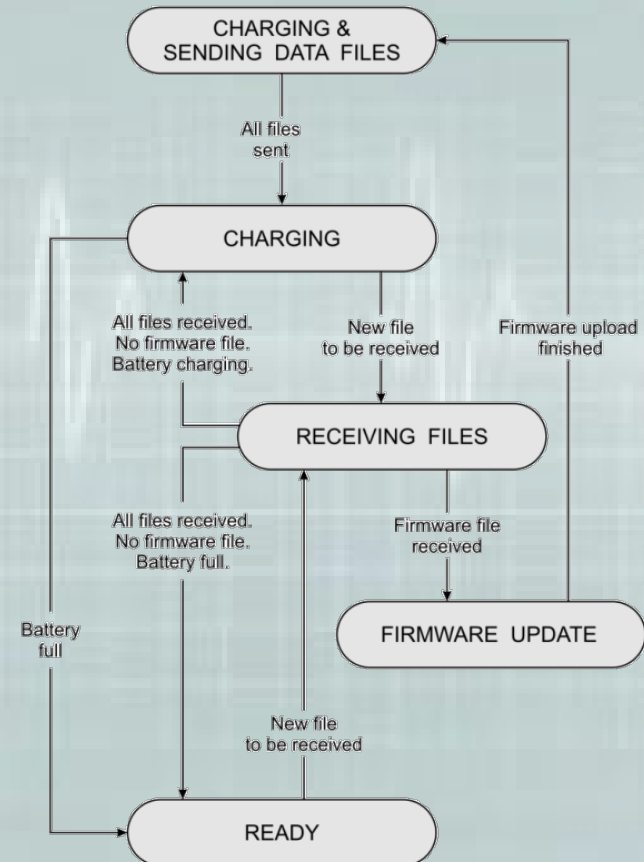


Smart Control – Bracel-AF state machine

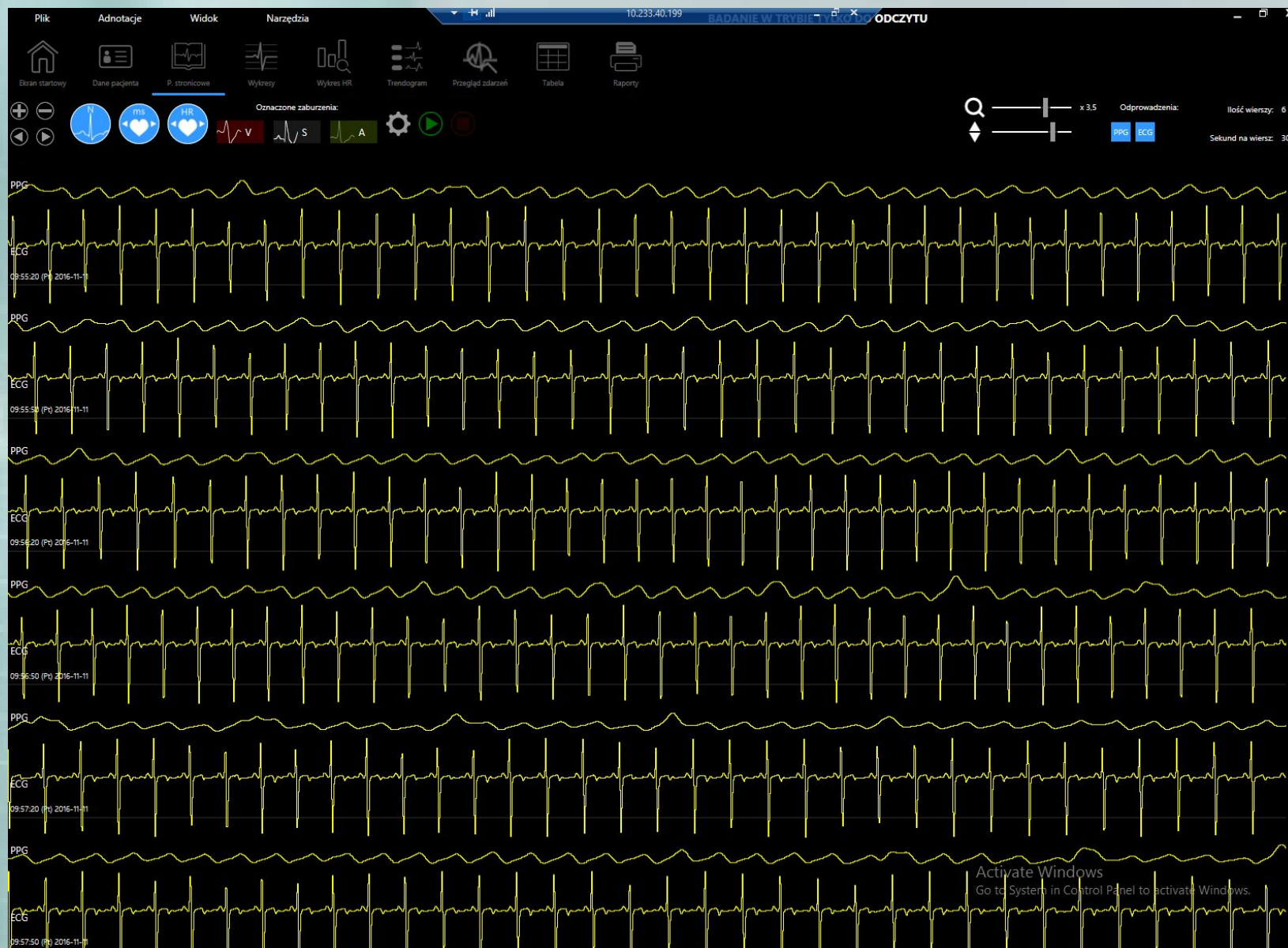
STATE: ACQUISITION



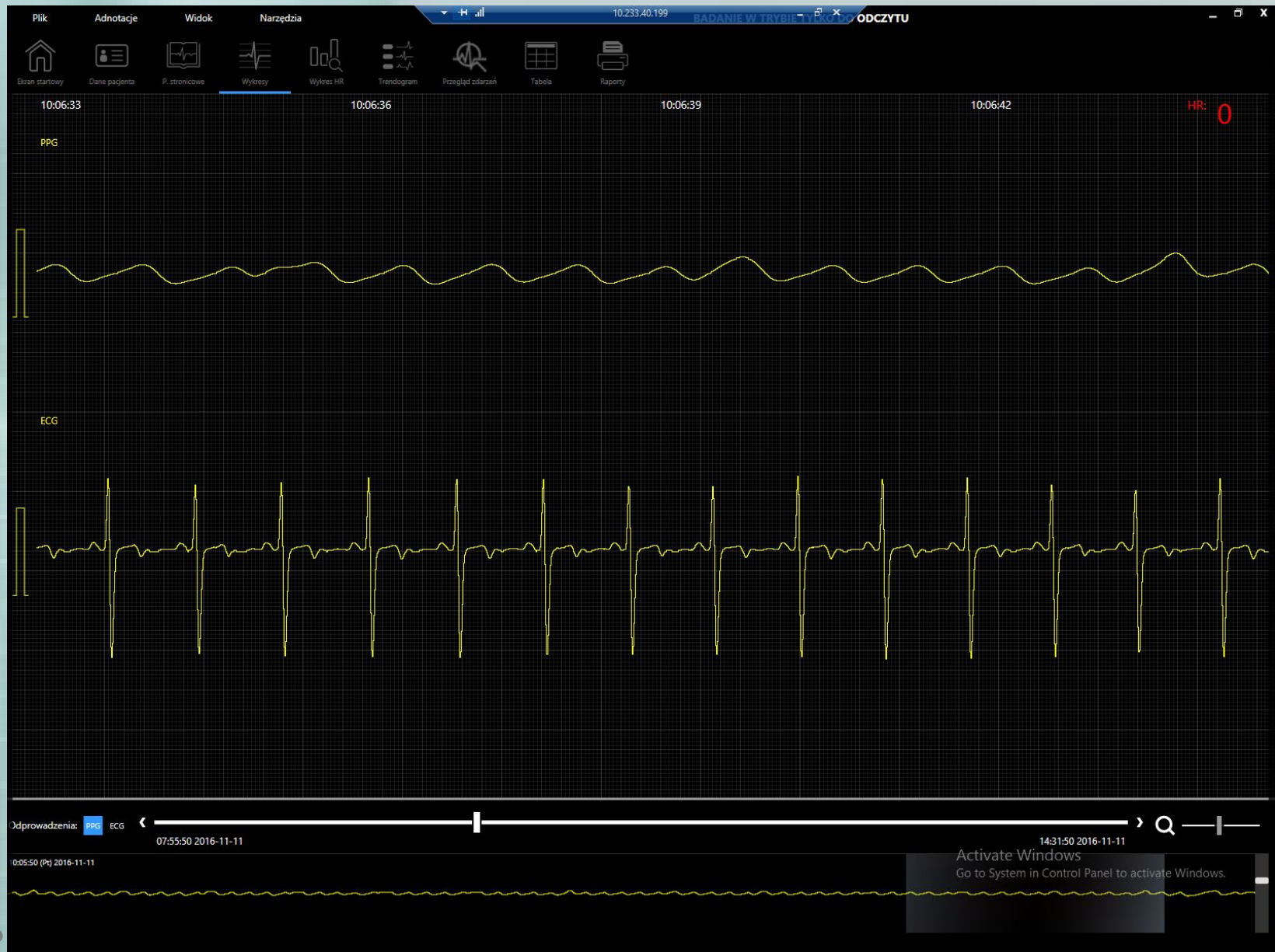
STATE: DOCKING



Para sygnałów PPG i EKG – Platforma Pacjenta



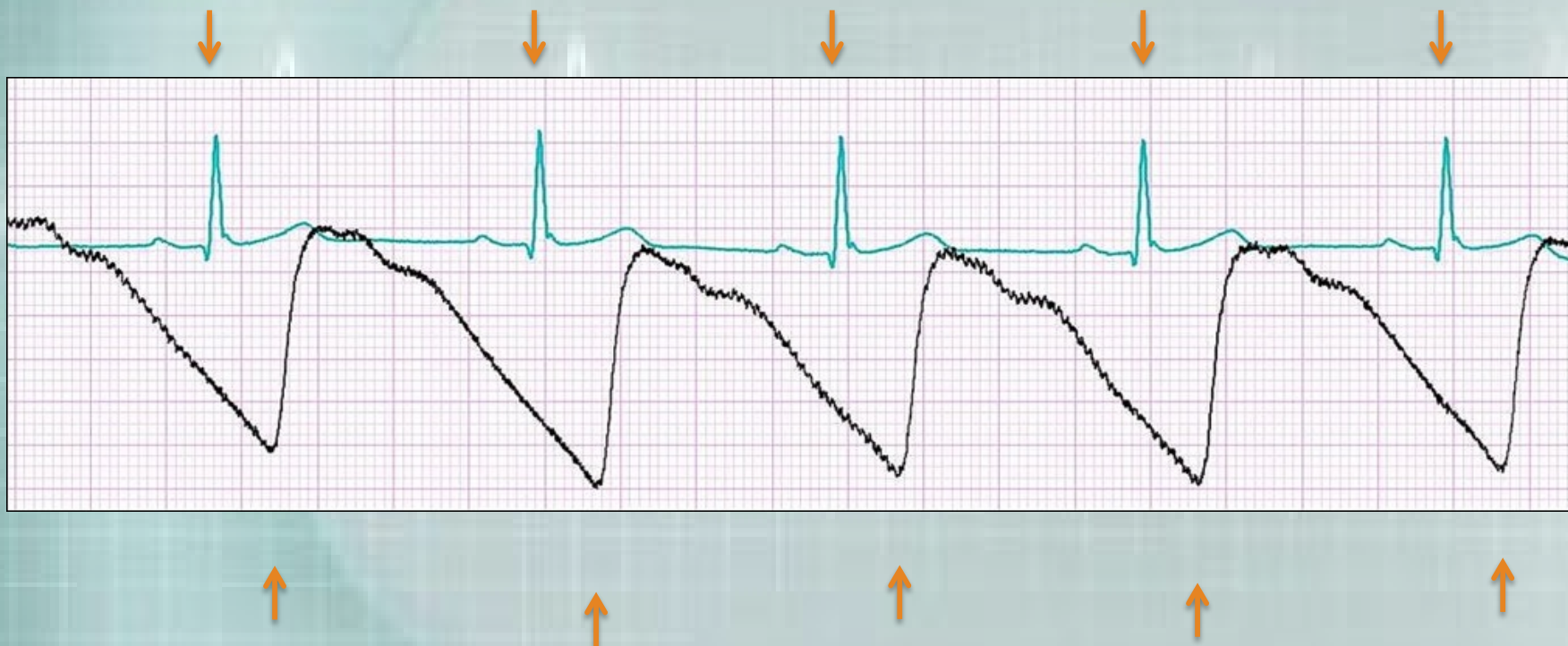
Stanisław U. 11.11.2016r.



Analiza sygnałów, wyznaczanie HR

Sygnały ECG i PPG – warunki idealne

100% zgodności HR z ECG i z PPG



Detekcja AF – ocena skuteczności



Opis bazy sygnałów:

The MIT-BIH Atrial Fibrillation Database (from PhysioNet.org)

This database includes **25** long-term ECG recordings of human subjects with atrial fibrillation. The individual recordings are each **10 hours** in duration. The original analog recordings were made at Boston's Beth Israel Hospital using ambulatory ECG recorders. The **rhythm annotation** files were prepared **manually by experts**; these contain rhythm annotations of types **AFIB** (atrial fibrillation), **AFL** (atrial flutter) and **N** (used to indicate all other rhythms).

*Goldberger AL, Amaral LAN, Glass L, Hausdorff JM, Ivanov PCh, Mark RG, Mietus JE, Moody GB, Peng C-K, Stanley HE. PhysioBank, PhysioToolkit, and PhysioNet: Components of a New Research Resource for Complex Physiologic Signals. Circulation **101**(23):e215-e220; 2000*

Detekcja AF – ocena skuteczności



The MIT-BIH Atrial Fibrillation Database ... ECG signals: All = 250h, AF = 106h

AF dev. – wyznaczone algorytmem ITAM	AF ref. – wzorcowe z bazy	
	AF ref. = 1	AF ref. = 0
AF dev. = 1	TP = 77,9h	FP = 6,6h
AF dev. = 0	FN = 6,7h	TN = 122,7h

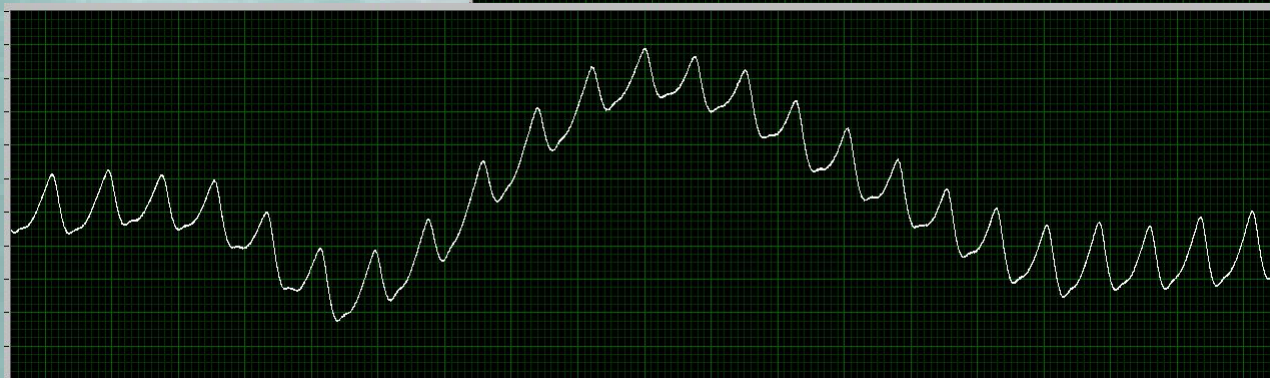
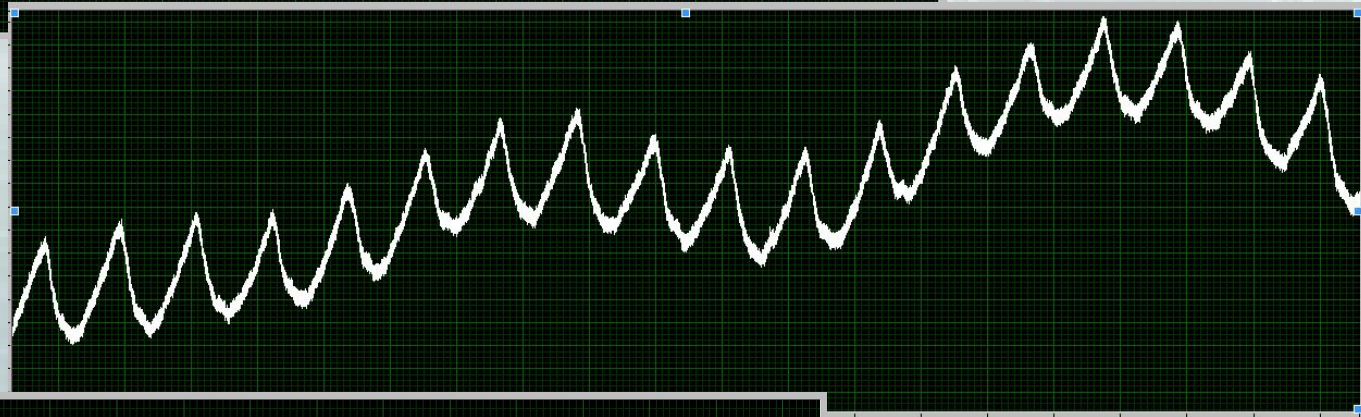
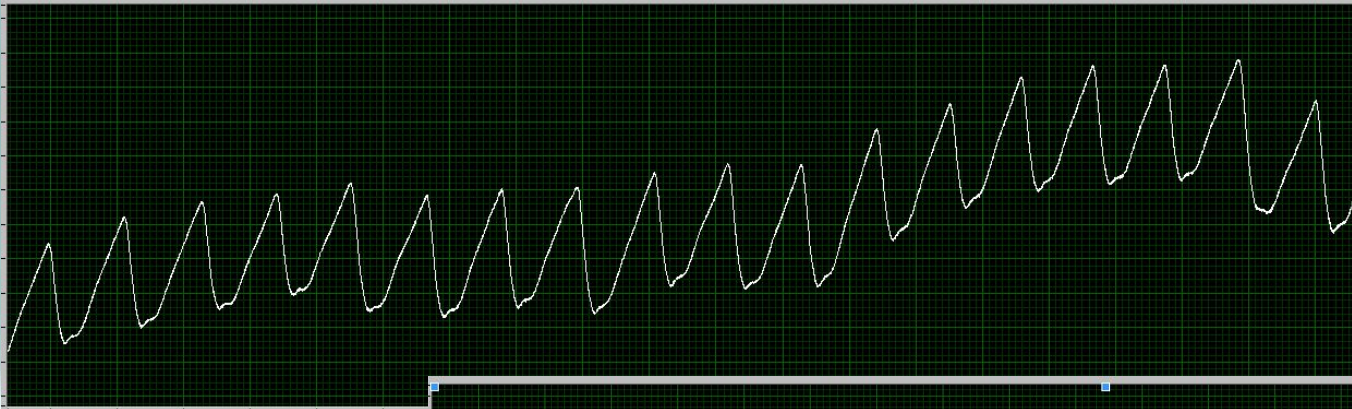
Skuteczność detekcji
93,7 %

Czułość = 92,0%

Swoistość = 94,9%

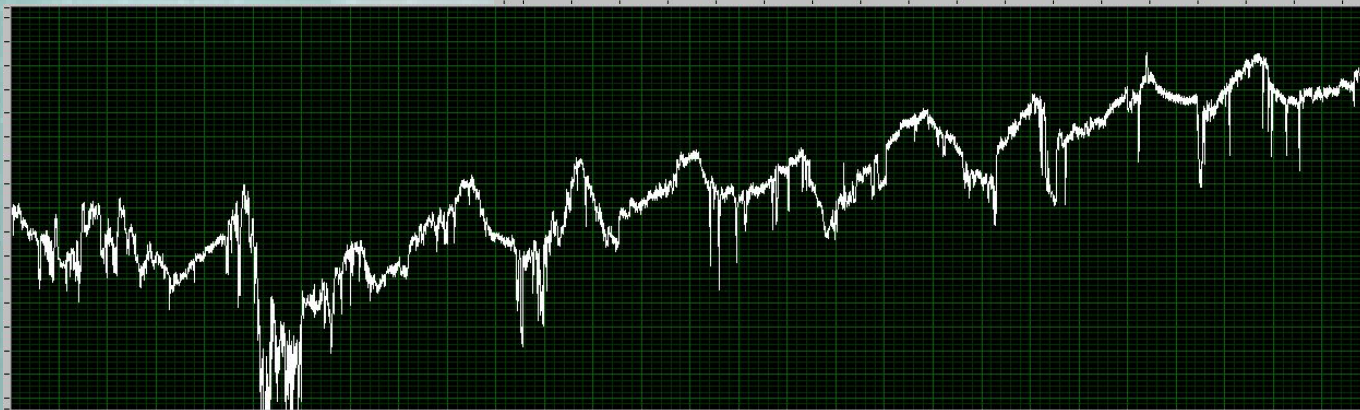
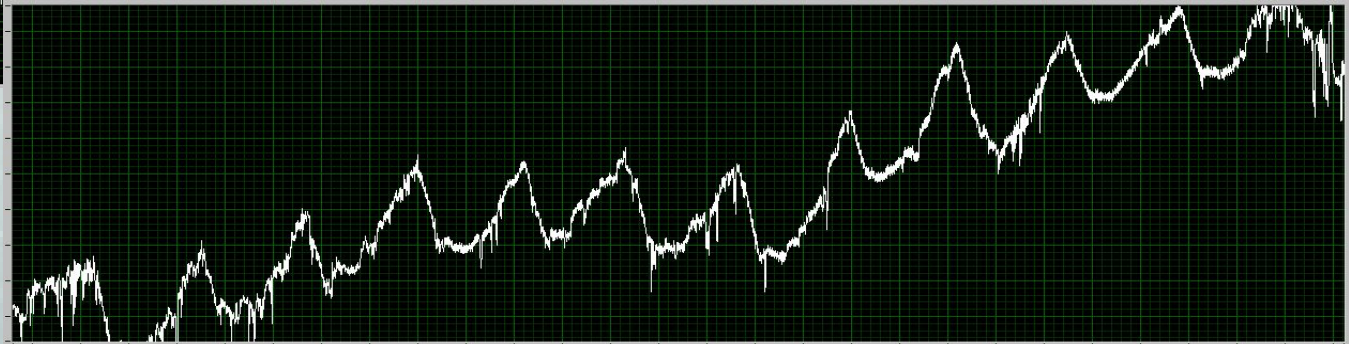
Analiza sygnałów, wyznaczanie HR

Sygnały PPG – dobra jakość



Analiza sygnałów, wyznaczanie HR

Sygnały PPG – niska jakość



Detekcja AF – wnioski

- Teoretyczna skuteczność detekcji okresów AF dla dobrej jakości sygnału PPG przy brak aktywności fizycznej osoby badanej przekracza 90%
- W skrajnym przypadku, przy wysokiej aktywności fizycznej bieg lub inne zajęcia sportowe, obsługa urządzeń mechanicznych istotnie się zmniejsza (nawet do kilkunastu procent)
- Rzeczywista skuteczność detekcji okresów AF w ciągu doby zależy od czas trwania podwyższonej aktywności fizycznej osób w grupie 65+

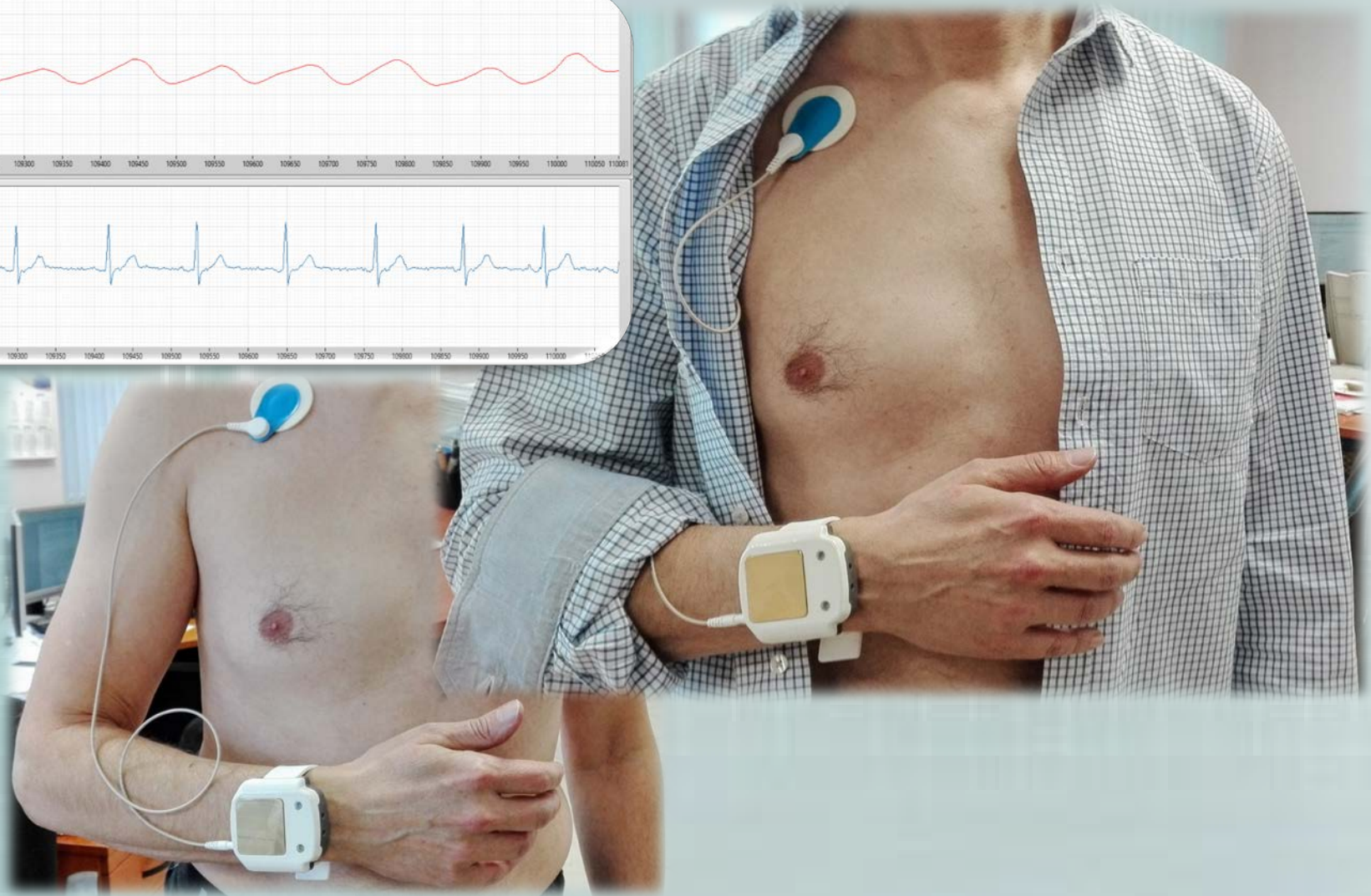
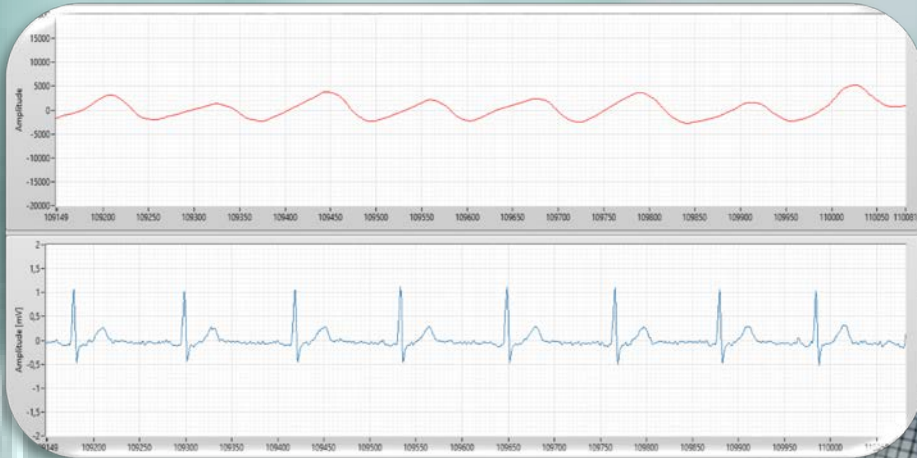
Wnioski z testów rejestratora bransoletkowego

- W listopadzie 2016 roku na posiedzeniu podsumowującym badania urządzeń Komitet Naukowy Projektu stwierdził, że zgodnie z obowiązującymi obecnie wytycznymi (“2016 ESC Guidelines for the management of atrial fibrillation developed in collaboration with EACTS”), wykrycie epizodu migotania przedsionków wymaga jego potwierdzenia w zapisie EKG. Oznacza to, że urządzenie monitorujące powinno zawsze w momentach wykrycia AF rejestrować jednocześnie sygnał EKG.
- Rejestrator bransoletkowy, którego działanie bazuje na analizie sygnału PPG, nie zawsze rejestruje sygnał EKG w momentach wykrycia epizodów AF (zależy to od dobrej woli pacjenta, który po sygnalizacji powinien przyłożyć palce drugiej ręki do elektrody rejestratora). Analiza przeprowadzonych sesji monitorowań wskazuje, że w rzeczywistych warunkach pacjenci (z różnych powodów) nie zawsze wykonywali tą czynność.
- Zaproponowano modyfikację urządzenia bransoletkowego wprowadzającą jednokanałowy zapis EKG metodą ciągłą (a nie tak jak dotychczas - na żądanie). Umożliwia to dołączenie do rejestratora bransoletkowego przewodu zakończonego elektrodą EKG klejoną w okolicy obojczyka.

Zmodyfikowana wersja rejestratora bransoletkowego

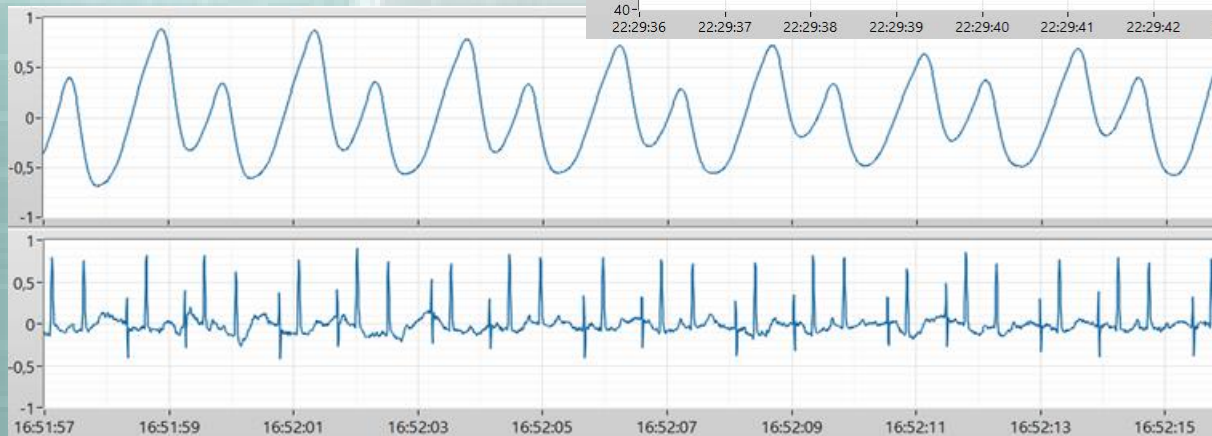
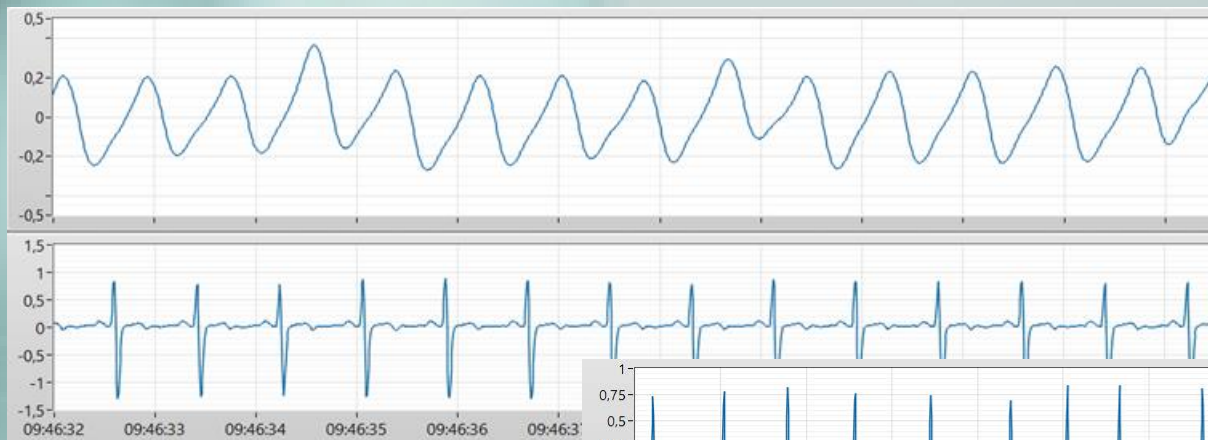


Przykład użycia rejestratora bransoletkowego



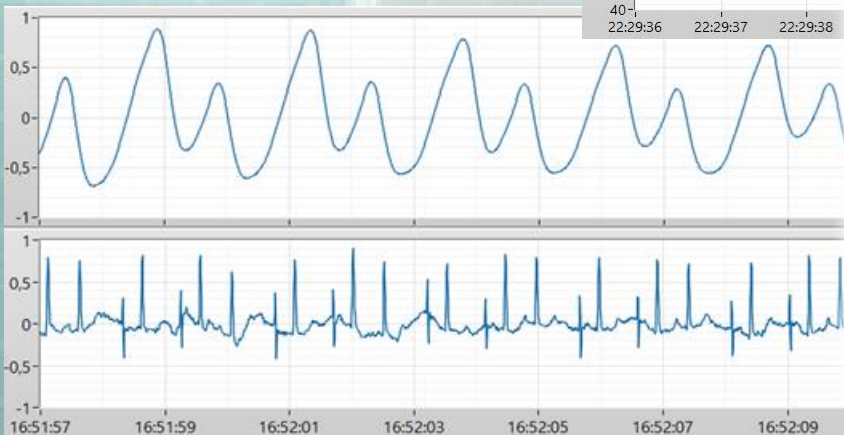
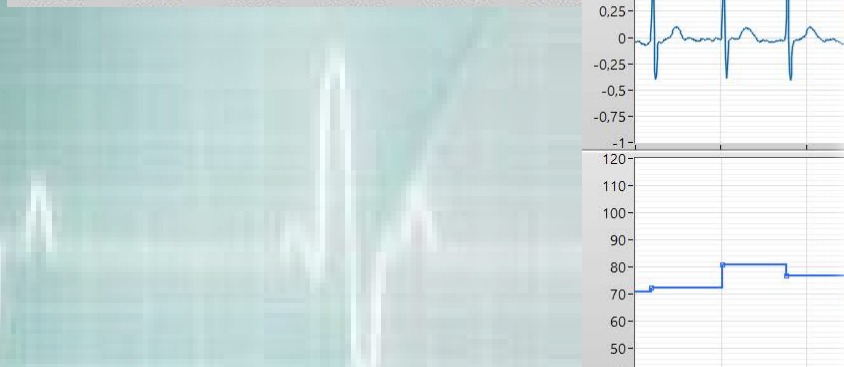
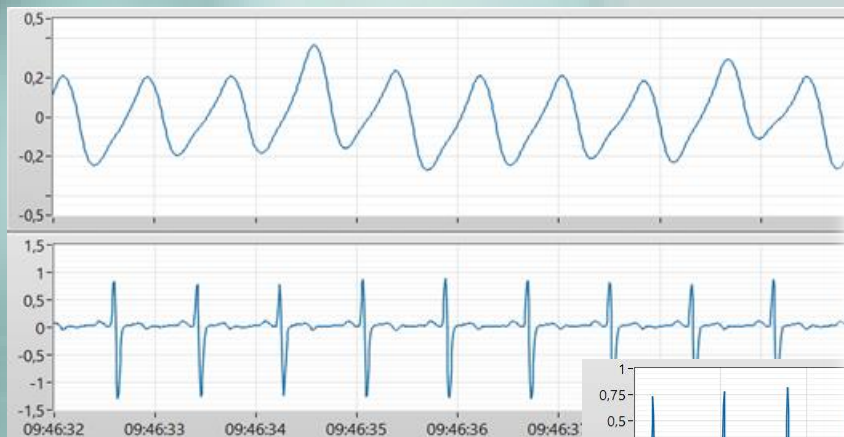
Wnioski i dalsze plany:

- Przeprowadzenie dalszych badań z modyfikowaną wersją rejestratora nadgarstkowego umożliwi ekstrakcję dodatkowych cech sygnału PPG (innych niż zmienność HR) charakterystycznych dla epizodów AF.
- Retrospektywna analiza zebranej bazy sygnałów umożliwi opracowanie nowych algorytmów ekstrakcji i klasyfikacji cech sygnału EKG i PPG dla potrzeb detekcji zjawiska migotania przedsionków.
- Uzyskane wyniki badań umożliwią wdrożenie i rozpowszechnienie, małych i nieuciążliwych dla pacjenta, urządzeń wykrywających migotanie przedsionków. Pozwoli to na objęcie monitorowaniem (screening) dużej grupy pacjentów bez konieczności korzystania z drogich i skomplikowanych w użyciu, wielokanałowych rejestratorów EKG.



Wnioski i dalsze plany:

- Pozyskane sygnały PPG zsynchronizowane z sygnałami EKG oraz uzupełnione o adnotacje informujące o wykryciu epizodów AF (przez eksperta klinicznego oraz urządzenie wszczepialne), będą stanowić unikalny zbiór danych, o dużej wartości naukowo-badawczej w obszarze medycyny i inżynierii biomedycznej.
- Tak przygotowane dane po zamieszczeniu w internetowym serwisie PhysioNet.org, udostępniającym różnorodne bazy sygnałów fizjologicznych, będą stanowić unikalną oraz powszechnie dostępną bazę wzorcową dla potrzeb badań naukowych.
To zapewni jej wysoką cytowalność w piśmiennictwie.



PHYSIONET RESEARCH RESOURCE FOR COMPLEX PHYSIOLOGIC SIGNALS

ABDOMINAL AND DIRECT FETAL ELECTROCARDIOGRAM DATABASE

<http://www.physionet.org/physiobank/database/adfecgdb/>

When referencing this material, please cite at least one of the following publications:

1. Jezewski J, Matonia A, Kupka T, Roj D, Czabanski R. >Determination of the fetal heart rate from abdominal signals: evaluation of beat-to-beat accuracy in relation to the direct fetal electrocardiogram. *Biomedical Engineering/Biomedizinische Technik* 2012 Jul;57(5):383-394. doi:10.1515/bmt-2011-0130.
2. Matonia A, Jezewski J, Kupka T, Horoba K, Wrobel J, Gacek A. The influence of coincidence of fetal and maternal QRS complexes on fetal heart rate reliability. *Medical & Biological Engineering & Computing* 2006;44(5):393-403.
3. Kotas M, Jezewski J, Horoba L, Matonia A. Application of spatio-temporal filtering to fetal electrocardiogram enhancement. *Computer Methods and Programs in Biomedicine*. 2011 Oct;104(1):1-9.
4. Kotas M, Jezewski J, Matonia A, Kupka T. Towards noise immune detection of fetal QRS complexes. *Computer Methods and Programs in Biomedicine*. 2010 Mar;97(3):241-256.

Please also include the standard citation for **PhysioNet**:

Goldberger AL, Amaral LAN, Glass L, Hausdorff JM, Ivanov PCh, Mark RG, Mietus JE, Moody GB, Peng C-K, Stanley HE. PhysioBank, PhysioToolkit, and PhysioNet: Components of a New Research Resource for Complex Physiologic Signals. *Circulation* 101(23):e215-e220 [Circulation Electronic Pages; <http://circ.ahajournals.org/cgi/content/full/101/23/e215>]; 2000 (June 13).

The research material included in the Abdominal and Direct Fetal Electrocardiogram Database contains multichannel fetal electrocardiogram (FECG) recordings obtained from 5 different women in labor, between 38 and 41 weeks of gestation. The recordings were acquired in the Department of Obstetrics at the Medical University of Silesia, by means of the KOMPOREL system for acquisition and analysis of fetal electrocardiogram (ITAM Institute, Zabrze, Poland). Each recording comprises four differential signals acquired from maternal abdomen and the reference direct fetal electrocardiogram registered from the fetal head.

Atrial Fibrillation Episodes Detection Based on Classification of Heart Rate Derived Features

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Krzysztof Horoba
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Hardware design issues and functional requirements for smart wristband monitor of silent atrial fibrillation

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Abstract—Atrial fibrillation (AF) is one of the most common cardiac arrhythmias and affects nearly 1.2% of every 100 persons

was to explore the possibility to classify heart beats into two classes describing the presence or absence of atrial fibrillation. Point of departure for the classification are features exclusively determined on the basis of heart intervals. The classification routine uses a linear model classifier and the performances are examined with the use of the MIT-BIH Atrial Fibrillation Database [57], [58].

II. ATRIAL FIBRILLATION EPISODES DETECTION

In this study, the AF detection is based on classification of features derived from the Heart Rate (HR). The last can be determined from ECG or Photoplethysmographic signal. Figure 1 presents an example of HR signal (upper part) with marked AF episodes (lower part).

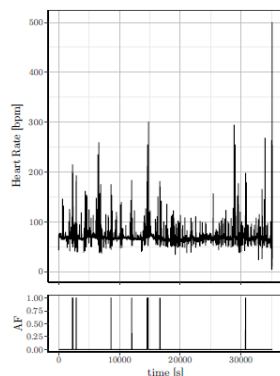


Fig. 1. Heart rate signal (upper part) with marked Atrial Fibrillation episodes (lower part).

The obvious advantages of considering the AF detection as a classification problem is the ability to separate the classifier from a variety of machine learning methods with varying degrees of complexity.

The next stage of this study aimed the definition and selection of features having the best ability to separate the two AF states. In a series of introductory simulations several possible features were investigated, and finally five of them were selected for further processing. The set of selected features,

besides the HR signal $x[i]$, $i = 1 \dots N$ itself (expressed in beat per minute (bpm)), includes:

- median value in a moving window of length $W = 2w + 1$, $w \in \mathbb{N} + \{0\}$

$$M(w)[i] = \text{median}\{x[i-w], \dots, x[i+w]\}, \quad (1)$$

- median absolute deviation from median in a moving window of length W

$$D(w)[i] = \text{median}\{|w[i-w], \dots, w[i+w] - M(w)[i]|\}, \quad (2)$$

- quantile of order p in a moving window of length W

$$Q_{(p,W)}[i] = \{z : \Pr(X(w)[i] \leq z) = p\}, \quad (3)$$

- where $X(w)[i]$ stands for the probability density function of $x[i]$ determined in a moving window of length W

- proportion of $x[i]$ in range $< i_1, i_2 >$ in a moving window of length W

$$P(w, i_1, i_2)[i] = \frac{\text{card}(G_i)}{W} \quad (4)$$

where

$$G_i = \{x_w[i] : x_w[i] \in [x[i-w], \dots, x[i+w]] \wedge x_w[i] \geq i_1 \wedge x_w[i] \leq i_2\}. \quad (5)$$

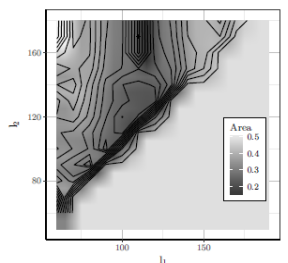


Fig. 2. Area of the overlapping part of probability density functions for $AF = 0$ and $AF = 1$ for feature $P(w, i_1, i_2)$ ($W = 21$)

The resulting feature set

$$\mathcal{F} = \{x[i], M(w)[i], D(w)[i], Q_{(p,W)}[i], Q_{(p,W)}[i], P(w, i_1, i_2)[i]\} \quad (6)$$

depends on a number of control parameters W , p , i_1 , i_2 . The control parameter values were determined in a series

In our AF monitor the AFE4403 module was used to drive green light-emitting diodes, as they offer a better signal quality when measuring just the pulse, compared to red or infrared light used in pulse oximetry. During normal operation the module switches between measurement of the reflected and ambient light intensity in each sampling cycle. Based on the average values of these two signals, obtained with the first order recursive filter, the intensity of the emitted light is being controlled (Fig. 3). Dedicated algorithm is designed to keep the average value of the signal at an optimal level of about 60% of the ADC measuring range, as well as to detect the situations where the recorder is not placed on the wrist.

D. On-demand ECG acquisition

The ECG measurement section of the presented AF monitor was based on ADS1292 integrated circuit (Texas Instruments). It is a specialized module for two-channel electrocardiographic acquisition. It is equipped with two low noise programmable gain amplifiers, internal reference voltage and a 24-bit sigma-delta converter. Additional functions include lead-off detection and flexible power management with standby and power-down modes. As being designed for mobile applications, the module is characterized by very low power consumption $\sim 35\mu\text{W}$ /channel. The placement of the analogue part and the A/D converter in one silicone structure results in high resistance to electromagnetic interferences [23]. Resistance to radio interference is also enhanced by EMI filters placed in analogue inputs inside the described structure.

Two silicon-carbon electrodes are placed on the top and bottom sides of the casing. The bottom electrode remains in contact with skin as long as the device is placed on the wrist, while the top electrode must be intentionally touched to enable the electrocardiogram acquisition.

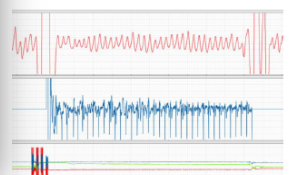


Fig. 4. PPG, ECG and ACC signals during the "on-demand" ECG acquisition. In the accelerometer signals clearly visible vibrations can be seen, requesting the patient to touch top electrode. Some distortions of the PPG signal can be noticed when patient touches and releases the electrode. Between these episodes a good quality ECG signal is acquired, with clearly visible, sharp QRS complexes.

Control and signal processing software embedded in smart wristband monitor of silent atrial fibrillation

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Recently carried out to gather reliable atrial fibrillation (AF) in elderly the project was focused on investing on in a form of wristband monitor, AF. The monitor

prevalence of silent AF and recognize the risk factors of silent AF in Polish population 65+. Additionally, positive validation results will allow us to develop a convenient and inexpensive system for widespread screening in order to detect silent AF

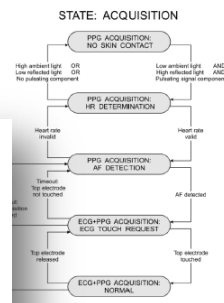


Fig. 5. FSM diagram of the signal acquisition state. Acquisition begins in "standby" state, and then, when a good signal quality is confirmed, the system state to "AF detection", being the most common for the state. In this state, two main transition sources are permitted, signal acquisition and detection of AF event.

On the other hand, the detection of AF event (detection of AF) leads to starting the ECG channel and signaling (by vibration) the request for touching the electrode. It is then that the patient will not be able to perform the measurement at once, because of working or other is such case, after 10 seconds, the program returns to a heart rate recording from photoplethysmogram and the atrial fibrillation events. If the patient touches the electrode and the electrical contact is detected, the recording measured (usually up to 30 seconds, which is the time enabling to confirm the atrial fibrillation from the PPG signal). Since the fibrillation is usually a short event, it was assumed that the registration request only after the AF occurs and disappears, so as to confirm the detection results basing on rhythmogram.

signal acquisition is terminated when the wristband is to the docking station. In turn, the communication is activated to establish communication link. First, the signal files are being sent to the docking station and, when confirmed, they are deleted from the device. Afterwards, the docking station is informed that all are already transmitted, and the mobile monitor is to charging state. In this state, the new firmware or update files may be uploaded to recorder according to update mechanism.

The mechanism was designed to update the firmware or update of all mobile monitors at the same time, in all the stations. When a new firmware version is released, it

is transmitted to all connected docking stations, typically working at the patients' homes. Every time a wristband is connected, the docking station checks its firmware version. Then all the signal files are transmitted, and finally, if a more recent firmware is available, the docking station sends the file to the monitor. The recorder recognizes the firmware file by its extension, and starts the bootloader program, located in a separate memory area. It erases the main program, replaces it by the new firmware and reboots the microcontroller. The configuration files, in turn, are just saved on the microSD card, since the configuration is read every time the program switches to Acquisition state.

C. Data Storage and Transmission

The data being acquired are saved to a file in a universal JHBD format, dedicated to multi-channel recorders of biophysical signals (Fig. 6). In this format the data are stored in a binary form, so the file size is optimized. The structure of the binary data is described in the header text using the JSON format. Thanks to this, the JHBD file can store the data from single- or multi-channel recorders, using any sampling frequency and any sample resolution. What's more, it is possible to save the data from channels of different bit resolution. In this way, a single file contains all the information needed for reading and visualization, including scale factors to convert the sample values into the physical quantities.

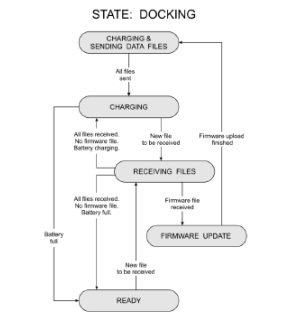
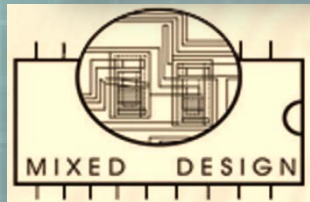


Fig. 6. FSM diagram of the signal docking state. When connected to docking station the charging process begins automatically (as it is managed by independent controller), and communication with docking station is established. First, all the acquired signal files are transmitted from the monitor to docking station. After that, any new configuration or firmware files are transmitted to the device.

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Podsumowanie:

- Opracowane, wytworzone i przetestowane w warunkach laboratoryjnych bransoletkowe urządzenie do detekcji epizodów niemego AF oparte na innowacyjnej i nieuciążliwej dla pacjenta metodzie pomiarowej, posiada duży potencjał badawczy i wdrożeniowy.
- Zastosowana metoda detekcji AF na podstawie cech krzywej pletyzmograficznej uzyskanej rejestratorem bransoletkowym stanowi rozwiązanie oryginalne i innowacyjne.
- Pozyskanie unikalnej bazy sygnałów PPG i EKG z referencyjnymi danymi z urządzeń wszczepialnych, istotnie podwyższy wartość naukowo-badawczą projektu w zakresie bioinżynierii.



Dziękuję za uwagę



Najnowsze doniesienia literaturowe:

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Background: Atrial fibrillation (AF) is a pathological condition leading to increased risk for embolic stroke and cardiac hospitalizations. Screening for AF represents a technical challenge because of the paroxysmal and frequently asymptomatic nature of the condition.

Objective: The aim was to investigate whether an unobtrusive **wrist-wearable device equipped with a photoplethysmographic (PPG) and acceleration sensors** could be used to detect AF.

Methods: **Sixteen patients** (M = 63%, age: **65.2 ± 14.0 y**, BMI: 29.7 ± 7.0 kg/m²) with suspected paroxysmal AF were monitored **for 24 hours** in outpatient setting using a portable ECG Holter recorder. Simultaneously, a wrist-wearable device equipped with a PPG and acceleration sensor was used to monitor heart rhythm and body movement. **PPG data were processed to extract the timing of heart beats** and derive inter-beat-intervals (IBI). **Acceleration data was used to discard IBI in presence of motion artifacts**. An ECG validated first-order Markov model was used to assess the probability of irregularly irregular rhythm of AF being present from PPG-derived IBI. AF detection outcome from the algorithm was compared with adjudications of AF episodes provided by clinical experts after visually inspecting ECG Holter data.

Results: Four patients experienced 100% AF burden, while 1 patient suffered from atrial flutter. The remaining patients showed normal sinus rhythm with several premature beats (808 supraventricular, range 0 – 4879; and 656 ventricular premature beats, range 0 – 4795). **AF detection was achieved with $97 \pm 2\%$ Sensitivity and $99 \pm 3\%$ Specificity**. During atrial flutter the algorithm output was non-AF 94.6% of the time. **Due to motion artifacts**, the algorithm **did not provide AF classification for $36 \pm 9\%$** of the 24 hours monitoring.

Conclusion: **A wrist-wearable device equipped with a PPG and acceleration sensor can provide accurate detection of rhythm irregularities caused by atrial fibrillation in free-living conditions.**